Faculty of Health: Medicine, Dentistry and Human Sciences

School of Psychology

2024-04

# Early-phase neuroplasticity induced by offline transcranial ultrasound stimulation in primates

#### Bault, N

https://pearl.plymouth.ac.uk/handle/10026.1/22442

10.1016/j.cobeha.2024.101370 Current Opinion in Behavioral Sciences Elsevier BV

All content in PEARL is protected by copyright law. Author manuscripts are made available in accordance with publisher policies. Please cite only the published version using the details provided on the item record or document. In the absence of an open licence (e.g. Creative Commons), permissions for further reuse of content should be sought from the publisher or author.



#### **ScienceDirect**



Review

## Early-phase neuroplasticity induced by offline transcranial ultrasound stimulation in primates\*

Nadège Bault 1,2,\*, Siti N Yaakub 1,2,\* and Elsa Fouragnan 1,2,\*



The use of 'offline' transcranial ultrasound stimulation (TUS) protocols is of particular interest in the rapidly growing field of low-intensity TUS. Offline TUS can modulate neural activity up to several hours after stimulation, suggesting the induction of early-phase neuroplasticity. Studies in both humans and nonhuman primates have shown spatially specific changes in both the neuromodulation target and in a distributed network of regions associated with it. These changes suggest that excitatory or inhibitory effects are a result of a complex interaction between the protocol used and the underlying brain region and state. Understanding how early-phase neuroplasticity is induced by offline TUS could open avenues for influencing late-phase neuroplasticity and therapeutic applications in a wide range of brain disorders.

#### Addresses

<sup>1</sup> Brain Research & Imaging Centre, Faculty of Health, University of Plymouth, Plymouth PL4 8BU, United Kingdom

<sup>2</sup> School of Psychology, Faculty of Health, University of Plymouth, Plymouth PL4 8AA, United Kingdom

Corresponding author: Bault, Nadège (nadege\_lab@nbault.net) \*Twitter account: @NadegeBault, @sitiny0, @EFouragnan

#### Current Opinion in Behavioral Sciences 2024, 56:101370

This review comes from a themed issue on Neurostimulation

Edited by Alex Sel and Elsa Fouragnan

For complete overview of the section, please refer to the article collection, "Neurostimulation (2023)"

Available online 8 March 2024

Received: 18 August 2023; Revised: 4 December 2023;

Accepted: 13 February 2024

https://doi.org/10.1016/j.cobeha.2024.101370

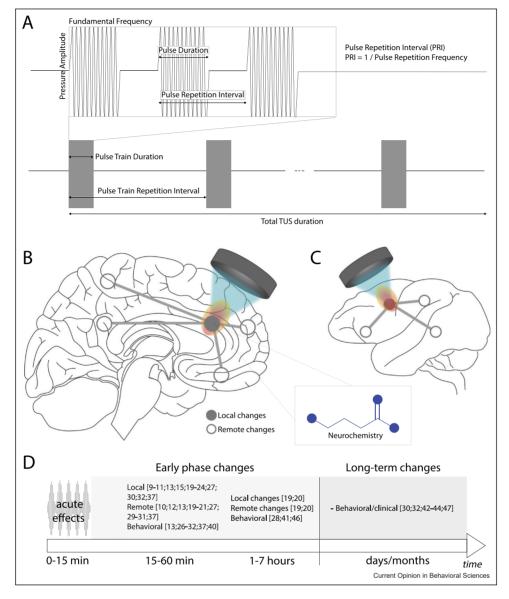
2352–1546/© 2024 The Authors. Published by Elsevier Ltd. This is an open access article under the CC BY license (http://creativecommons.org/licenses/by/4.0/).

#### Introduction

Adaptive neuroplasticity is integral both in correcting or improving aberrant function in a large range of neurological and psychiatric disorders and in ensuring normal functioning in healthy ageing. Measuring and inducing neuroplasticity can thus be beneficial therapeutically and can also improve our understanding of the brain in general health [1]. Brain stimulation, or more generally, neuromodulation methods, can elicit functional brain changes and thereby promote neuroplasticity [2]. Recently, transcranial ultrasound stimulation (TUS) applied at low intensity has been found to safely induce neuronal changes with high spatial specificity in both superficial cortex and deep brain regions [3,4] when careful considerations are taken to limit the transmission loss caused by the skull [5]. TUS uses acoustic energy to mainly leverage the mechanosensitivity of neural tissue to bring about changes in neuroplasticity [6,7].

TUS protocols can be categorised into online or offline according to the duration of their effects. The term 'online' refers to TUS protocols aimed at triggering acute effects, which occur only during or immediately after the neuromodulation period. These online interventions, particularly in humans, usually involve pulse trains that do not last more than half a second (see Figure 1a and legend for TUS parameter definition). These are hypothesised to change the underlying brain activity of the region targeted, with some evidence for network changes but produce no lasting effects beyond the stimulation period itself. 'Offline' TUS protocols on the other hand aim to induce effects that significantly outlast the stimulation period, for example, by minutes or hours, even days, after the intervention. These protocols are usually characterised by long duration pulses or trains of pulses that typically last 20 s or longer. These are thought to induce both local and distributed changes across the whole brain. There is an ongoing debate in the TUS community about the presence of sensory costimulation (e.g. the sound that accompanies TUS protocols) and how this may influence the effects of TUS [8]. While the delayed readout in offline studies reduces the risk of such issues, placebo/nocebo effects could still be based on both participants' and researchers' expectations. These issues can be mitigated by introducing good study control and double-blinding procedures (see Table 1).

<sup>\*</sup> Given the role as Guest Editor, Elsa Fouragnan had no involvement in the peer review of the article and has no access to information regarding its peer review. Full responsibility for the editorial process of this article was delegated to Alex Sel.



Schematic of an ultrasound pressure waveform and illustrations of some of the offline TUS effects presented in this review. (a) A rectangular ramp shape is used to present the pressure amplitude. Typically, the positive and negative amplitudes are the same when operating at low pressures, to be within the linear regime. A single continuous sonication is a pulse and has a duration of PD. Pulses are often repeated in a pulse train. The duration between two pulses in a pulse train is the pulse repetition interval and is equal to 1 divided by the PRF. The pulse train will have a duration, which is the pulse train duration. The pulse train can be repeated and, if so, has a structure similar to the pulse. (b) Local and remote effects in humans, including changes in neurochemistry. (c) Local and remote effects in nonhuman primates. (d) Summary of the timescale of effects following offline TUS.

In this review, we will explore the ability of offline TUS, in primates, to induce changes in behaviour and neural activity that outlast the sonication period by minutes, hours, or even days, covering papers up to August 2023. We will then discuss whether the observed effects can be related to changes in synaptic strength (i.e. synaptic plasticity) and induction of long-term effects. This is crucial to lay the groundwork for translating offline TUS protocols into clinical interventions in which TUS will produce long-lasting therapeutic changes.

#### Measuring TUS-induced neuroplasticity

The effects mediated by offline TUS include both local and remote neuronal changes (Figure 1a and b) as well as changes in behaviour related to specific cognitive engagement and in their associated neural correlates. These changes occur in the minutes, hours, or days following TUS (Figure 1c). These changes could be induced when subjects are at rest or under anaesthesia or could be evoked by using another brain stimulation method or by engaging in a behavioural task. The same

Table 1									
Summary of	offline TUS p	Summary of offline TUS protocols used in primate studies included in this review.	nate studies inclu	uded in this review.					
Paper	Species	Condition, state	Readout	Brain area	Transducer placement	Evaluation of stimulation efficacy/target engagement	Controls	Blinding	TUS protocol: FF; PD; PRF; duration; repetition (if any)
Monti et al., 2016 [43]	Human	Disorder of consciousness, not awake	Behaviour	Thalamus	MR guided	No	O N	P blind state R not blind	FF = 650 kHz; PD = 0.5 ms; PRF = 100 Hz; duration = 30 s; Repeated every 30 s over a period of 10 min
Badran et al., 2020 [40]	Human	Healthy, awake	fMRI	Thalamus	MR guided	ON.	No stim.	P blind- R blind collection and	FF = 650 kHz; PD = 5 ms; PRF = 10 Hz; duration = 30 s; Repeated every 30 s over a period of 10 min
Reznik et al., 2020 [42]	Human	Depression, awake	Behaviour	Frontotemporal	Not reported	k-Wave and example CT	No stim.	P blind- R blind collection	FF = 500 kHz; PD = 0.065 ms; PRF = 40 Hz; duration = 30 s
Sanguinetti et al., 2020 [41]	Human	Healthy, awake	fMRI	Inferior frontal gyrus	Localiser cap	k-Wave and example CT	No stim.	P blind- R blind collection	FF = 500 kHz; PD = 0.065 ms; PRF = 40 Hz; duration = 30 s
Cain et al., 2021 [12]	Human	Healthy, awake	fMRI; ASL	Globus pallidus	MR guided	k-Wave and example CT	<u>0</u>	R not blind R not blind	Low PRF protocol: FF = 650 kHz; PD = 5 ms; PRF = 10 Hz; duration = 30 s; Repeated every 30 s for 10 min; High PRF protocol: FF = 650 kHz; PD = 0.5 ms; FF = 100 Hz; duration = 30 s; Repeated every 30 s for 10 min
Cain et al., 2021 [44]	Human	Disorder of consciousness, not awake	Behaviour	Thalamus	MR guided	o :		P blind state R not blind	FF = 650 kHz; PD = 0.5 ms; PRF = 100 Hz; duration = 30 s; Repeated every 30 s for 10 min
Zhang et al., 2021 [22]	Human	Healthy, awake	TMS; behaviour M1 hand	M1 hand	TMS-MEP hotspot	k-Wave and example anat.	No stim.	P blind- R not blind	FF = 500 kHz; PD = 500 µs; PRF = 100 Hz; duration = 500 ms; Repeated every 8 s for 15 min
Lee et al., 2022 [47]	Human	Epilepsy, awake	Stereo EEG; seizure monitoring	Seizure onset zone	MR guided	k-Wave and indiv. CT	<u>.</u> E	P blind R not blind	FF = not reported; PD = 3 ms; PRF = 100 Hz; duration = 10 min
Nakajima et al., 2022 [37]	Human	Healthy, awake	fMRI; behaviour	M1 hand, STN, putamen, alFC, middle frontal cortex	Neuronav. indiv. struct. MRI	k-Wave and indiv. struct. MRI	Active in study 3 only	P not blind R not blind	FF = 500 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s
Samuel et al., 2022 [16]		Healthy, awake	TMS; MEG	M1 hand	TMS-MEP hotspot	o <sub>N</sub>		P not blind R not blind	FF = 500 kHz; PD = 20 ms; PRF = 5 Hz; duration = 80 s
Zeng et al., 2022 [23]	Human	неагту, аwаке	SS W	M1 hand	IMS-MEP hotspot	o Z	Sham and active	P not blind R not blind	Low PHF protocol: FF = 500 kHz; PD = 20 ms; PRF = 5 Hz; duration = 80 s High PRF protocol: FF = 500 kHz; PD = 0.32 ms; PRF = 1000 Hz; duration = 80 s; Repeated every 1.1 s for 55 s

Table 1 (continued)	tinued)								
Paper	Species	Condition, state	Readout	Brain area	Transducer placement	Evaluation of stimulation efficacy/ target engagement	Controls	Blinding	TUS protocol: FF; PD; PRF; duration; repetition (if any)
Chou et al., 2023ª	Human	Healthy, awake	fMRI; pain response	Amygdala	Not reported	No	No stim.	P not blind R not blind	Not reported
Kuhn et al., 2023 [13]	Human	Healthy, awake	fMRI; ASL	Amygdala, entorhinal cortex	MR guided	Prior water tank measurements and skull	Active	P blind+ R blind collection and analyses	Amygdala protocol: FF = 650 kHz; PD = 5 ms; PRF = 10 Hz; duration = 30 s; Repeated every 30 s for 5 min Entruhinal cortex protocol:
									FF = 650 kHz; PD = 0.5 ms; PRF = 100 Hz; duration = 30 s; Repeated every 30 s for 5 min
Ren et al., 2023 [24]	Human	Healthy, awake	TMS	M1 hand	Localiser cap	O V	No stim.	P not blind R not blind	FF = 500 kHz; PD = 500 µs; PRF = 100 Hz; duration = 500 ms Repeated every 8 s for 15 min
Yaakub et al., 2023 [10]	Human	Healthy, awake	fMRI; MRS	PCC, dACC	Neuronav. indiv. struct. MRI	k-Wave and indiv. struct. MRI	Sham and active	P blind+ R not blind	FF = 500 kHz; PD = 20 ms; PRF = 5 Hz; duration = 80 s
Zhang et al.,	Human	Healthy, awake	TMS; MRS	M1 hand	Neuronav.	Water tank		P not blind	Low PRF protocol:
2023 [11]					indiv. struct. MRI	measurements and skull Onscale and	y 1 itrols ies 2	R not blind	FF = 500 kHz; PD = 400 μs; PRF = 50 Hz; duration = 500 ms; Repeated every 2 s for 5 min
						example CTs	and 3		High PRF protocol: FF = 500 kHz; PD = 200 µs; PRF = 2000 Hz; duration = 500 ms; Repeated every 2 s for 5 min
Verhagen et al.,	Rhesus macaque	Healthy, sedated	fMRI	Frontal polar cortex	Neuronav. indiv.	Custom and example CT	No stim. and active	P blind state R not blind	FF = 250 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s
2019 [19] Folloni et al., 2019 [20]	Rhesus macaque	Healthy, sedated	fMRI	pACC; amygdala	struct. Mrs. Neuronav. indiv.	Custom and example CT	No stim. and active	P blind state R not blind	FF = 250 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s
Fouragnan et al., 2019 [28]	Rhesus macaque	Healthy, awake	fMRI	pACC	Neuronav. indiv. struct. MRI	Custom and example CT	No stim. and active	P blind state R not blind	FF = 250 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s
Khalighinejad et al., 2020 [29]	Rhesus macaque	Healthy, sedated	fMRI	Basal forebrain	Neuronav. indiv. struct. MRI	Custom and example CT	No stim. and active	P blind state R not blind	FF = 250 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s
Pouget et al., 2020 [31]	Rhesus macaque	Healthy, awake	Behaviour	FEF	Neuronav. indiv. struct. MRI	k-Wave and example CT	No stim. and active	P blind state R not blind	FF = 320 kHz; PD = 30 ms; PRF = 10 Hz; duration = 20 s
Zou et al., 2020 [46]	Rhesus macaque	Epilepsy model, awake	Video EEG	M1 hand	Not reported	Water tank measurements and skull	No stim.	P blind state R not blind	FF = 800 kHz; PD = 0.555 ms; PRF = 500 kHz; duration = 15 min
Bongioanni et al., 2021 [26]	Rhesus macaque	Healthy, awake	Behaviour	Medial frontal cortex	Neuronav. indiv. struct. MRI	0 Z	No stim. and active	P blind state R not blind	FF = 250 kHz; PD = 30 ms; PRF = 10 Hz; duration = 40 s

Table 1 (continued)	ntinued)								
Paper	Species	Condition, state	Readout	Brain area	Transducer placement	Evaluation of stimulation efficacy/target engagement	Controls	Blinding	TUS protocol: FF; PD; PRF; duration; repetition (if any)
Folloni et al., Rhesus 2021 [27] macaqu	Rhesus macaque	Healthy, awake	fMRI; behaviour Lateral OFC; anterior PFC	Lateral OFC; anterior PFC	Neuronav. indiv. struct. MRI	Custom and example CT	No stim. and active	P blind state R not blind	P blind state FF = 250 kHz; PD = 30 ms; R not blind PRF = 10 Hz; duration = 40 s
Munoz et al., Rhesus 2022 [30] macaqu	Rhesus macaque	Healthy, awake	fMRI	Striatum	Neuronav. indiv. struct. MRI	N <sub>O</sub>	No stim. and active	P blind state R not blind	FF = 500 kHz; PD = 10 ms; PRF = 2 Hz; duration = 2 min
Liu et al., 2023 [21]	Nonhuman primate (unspecified)	Healthy, sedated	fMRI	Caudate nucleus	Neuronav. template	k-Wave and example CT	No stim.	P blind state R not blind	FF = 500 kHz; PD = 10 ms; PRF = 2 Hz; duration = 2 min
Webb et al., 2023 [32]	Rhesus macaque	Healthy, awake	Intracranial EEG; behaviour	<b>LGN</b>	Custom head frame	MR thermometry	Sham and active	P blind state R not blind	FF = 480 kHz; PD = 30 ms; PRF = variable; duration = 30 s; Repeated daily for more than 6 months

'Neuronav. template', example stereotaxic neuronavigation system, tracked continuously with infrared reflectors, using a template MRI structural image. 'MR guided', iterative transducer placement using MRI of the transducer position on scalp. 'Localiser cap', transducer positioned using electrode position on EEG cap or scalp distance measurements. 'TMS-MEP hotspot', point ransducer placement: 'Neuronav. indiv. struct MRI', stereotaxic neuronavigation system, tracked continuously with infrared reflectors, using participant's MRI structural (T1-weighted) image frontal eye field; OFC, orbitofrontal cortex primary motor cortex; aIFC, anterior inferior frontal cortex; dACC, dorsal ACC; pACC, perigenual ACC; FEF, on scalp associated with highest MEP after TMS stimulation. Brain area: M1,

Evaluation of stimulation efficacy/target engagement: 'example GT/example anat.', simulation run using a template/example CT scan(s) or an example MRI anatomical image(s) converted into a

pseudo-CT(s). 'k-Wave/custom indiv. CT/struct. MRI', individual simulations run with k-wave or custom scripts, using the participant's CT or MRI anatomical image converted into a pseudo-CT

not blinded or blinding procedure not reported. 'P blind state', participant is nonhuman primate or human in a minimally conscious state. 'R blind collection', researcher blinding during data Blinding: 'P blind+', participant blinding with successful postcheck. 'P blind-', participant blinding attempted with unsuccessful postcheck or failure to control for sound. 'P not blind-', participant or replicating stimulation sound using bone-Controls: 'Active', active control brain region. 'Sham', sham control including sound control (unfocused stimulation, sound masking, white noise, conducting headphones). 'No stim.', control session without simulation or sham control excluding sound control. No, no control session/group. 'Water tank measurements & skull', water tank measurements using a hydrophone and *ex vivo* skull in degassed water

collection. 'R blind collection and analyses', researcher blinding during data collection and analyses. 'R not blind', researcher not blinded or blinding procedure not reported

TUS protocol: FF, fundamental frequency; PD, pulse duration. Abstract 38 in Biological Psychiatry 2023, 93:S84-S85. effects have also been investigated with online TUS (for a review on online TUS effects, please see Refs. [7,9]).

Taking advantage of their high spatial specificity, a range of noninvasive neuroimaging methods have been used to assess local and remote neuronal effects of offline TUS in primates (Figure 1a and b). These effects include, but are not limited to, local and global changes in blood flow-related brain activity and connectivity (task-based and resting-state functional magnetic resonance imaging [fMRI]), metabolite concentrations (magnetic resonance spectroscopy [MRS]), and perfusion (arterial spin labelling [ASL]). With higher temporal resolution, magnetoencephalography (MEG) and electroencephalography (EEG) allow the investigation of time-frequency-dependent brain activity, and the temporal dynamics of changes in brain oscillations induced by TUS. Offline TUS can also be coupled with other forms of brain stimulation, such as transcranial magnetic stimulation (TMS) to modulate another form of evoked response, for example, motor evoked potentials (MEP) induced by TMS.

In the absence of neuroimaging or additional neurostimulation methods to quantify measures of neuroplasticity, TUS can simply be used to impact behavioural or cognitive functioning, arguably the ultimate output of network activity. However, unlike other brain stimulation methods, there is currently no evidence that TUS can elicit readily observable behavioural readouts that can confirm target engagement (e.g. a finger twitch, as elicited by TMS of the hand area of the motor cortex). With higher order cognition, behavioural readout becomes less informative regarding TUS target engagement. In these cases, some other method for inferring target engagement can be useful, for example, through acoustic simulations.

#### Evidence supporting local changes

Techniques for investigating the local impact of offline TUS include assessing changes within the anatomically defined brain region at the location of the peak intensity of TUS or within specified boundaries of the acoustic pressure field of the TUS. Two human studies used MRS to measure the concentration of γ-aminobutyric acid (GABA), the main inhibitory neurotransmitter, in a voxel broadly overlapping with the TUS focal pressure field [10,11]. Using a low pulse repetition frequency (PRF) TUS protocol (5 Hz) targeted on the posterior cingulate cortex (PCC; see Table 1 for details on all protocols), Yaakub et al. observed a decrease in the concentration of GABA in the PCC but not in the dorsal anterior cingulate cortex (ACC), indicating a spatially specific increase in excitability in the hour following TUS [10]. Revealing longer lasting effects, Zhang et al. [11] found that both excitatory and inhibitory effects of TUS on GABA levels in the motor cortex depend on the

type of TUS protocol applied. With repeated sonication over 7 days, the effects can persist for up to 24 hours. Using ASL, one study [12] found a decrease in perfusion, indicating inhibition, after stimulating the basal ganglia, while another [13] reported an increase in perfusion following amygdala and entorhinal cortex stimulation. These seemingly contradictory inhibitory and excitatory effects may indicate complex relationships between TUS protocols, tissue composition, and states [14,15].

### Evidence supporting spatial specificity of distributed network changes

The effects of offline TUS can be observed not just locally, at the site of stimulation, but in a network of regions associated with the stimulation site. Using a low PRF protocol (5 Hz), TUS applied to the human motor cortex has been found to not only change MEG alpha power in the motor cortex and increase local MEG connectivity within the motor areas but also affect beta power in functionally connected regions up to 25 min post-TUS [16]. Confirming the intricate offline TUS impact on brain networks, multiple nonhuman primate studies found significant changes in coupling between the sonicated region and its functionally relevant neural network or 'connectivity fingerprint' [17,18]. These studies showed that TUS of specific deep cortical and subcortical regions, while the animals were under anaesthesia, perturbed the connectivity profile of the sonicated region up to 2 hours after TUS. These effects were regionally specific: sonication of distinct regions of the medial frontal cortex caused changes in each area's connectivity fingerprint only when TUS was applied to the area itself, and not to a control region [19], even when the two brain areas are only a few millimetres apart [20]. This was confirmed in another nonhuman primate study targeting the caudate nucleus with a lower PRF protocol [21] (2 Hz PRF instead of 10 Hz PRF in the previous two studies [19,20]). In humans, the same was observed after TUS of the dorsal ACC and PCC were performed [10], with these changes showing a time dependence where functional connectivity of the target region was initially limited to a small network of regions during the early fMRI acquisition (at approximately 13 min post-TUS), with later changes (at approximately 46 min post-TUS) involving a larger network of regions.

#### Modulation of evoked response

Neuroplasticity induced by TUS may also include excitability or inhibitory effects that can be measured with TMS (e.g. TMS-induced MEP). In a series of work combining offline TUS and TMS in humans, MEP amplitudes were amplified by repetitive low PRF offline TUS (PRF range 5–100 Hz; see Table 1 for details of the protocols) [22–24]. Facilitatory effects were still present 30 min postsonication in one study [24], confirming the duration of offline TUS effects on neural transmission.

Contrasting with these results, Zhang et al. [11] found excitatory effects in the form of decreased intracortical inhibition produced by a high PRF protocol (2000 Hz) and inhibitory effects — reduced MEP amplitudes, increased intracortical inhibition and decreased intracortical facilitation — with a lower PRF protocol (50 Hz). Drawing a conclusion about the impact of PRF on excitation and inhibition from these studies is difficult as other TUS parameters also differed between the studies. Furthermore, the latter study [11] was the only one (of the four reported here) to use stereotaxic neuronavigation and acoustic simulation to ensure more accurate and efficient targeting of M1. As the effect of specific protocol parameters on the type and duration of offline effects is still poorly understood, the field would benefit from further systematic exploration of the parameter space.

#### Nonhuman primates: task-related changes and associated brain networks

The ability of TUS to induce neuronal changes in the targeted region and its associated network that outlast the stimulation itself can open vast avenues to elucidate brain-behaviour relationships. As such, offline TUS can be used to modulate performance during a cognitive task following TUS intervention [25]. In nonhuman primates, a low PRF protocol (10 Hz) has been found to perturb activity in specific parts of the frontal cortex [26–28] and basal forebrain [29], but not adjacent brain regions. This manipulation had direct effects on behaviour, revealing the causal role of the perigenual ACC in translating cue information into choices [28], of the area 47/120 in credit assignment [27], of the basal forebrain in altering the timing of decisions [29] and of the medial frontal cortex in estimating novel choice values [26]. Another low PRF offline protocol (2 Hz) also modified motivational and cognitive aspects of behavioural performance in a motivated decision-making task [30].

In addition to perturbing high-level decision-making processes, offline TUS can interfere with perceptual processes. Using a saccade task, TUS directed to oculomotor regions perturbed saccade latencies up to 20 min postsonication [31]. During a visual discrimination task, offline TUS applied to the lateral geniculate nucleus (LGN) produced a choice bias towards the contralateral hemifield peaking 15 min after TUS with an increase in gamma activity measured with intracranial EEG. Surprisingly, and questioning the possibility for longer-term changes in neuroplasticity, the TUS-induced bias reduced over the course of 5 months of daily sessions due to adaptation, although the effect did reappear after the first TUS session following a 1-month break [32].

#### Task-related changes in humans

The large majority of human studies targeting task-dependent cognitive processes make use of online TUS protocols to find acute TUS-evoked effects [8,33-36]. Nevertheless, the efficacy of offline stimulation in changing behaviour over time and beyond the stimulation period itself is beginning to be established. Offline TUS of the anterior putamen, subthalamic nucleus (STN), and inferior frontal cortex caused a sustained disruption of motor response inhibition during a stopsignal task, effective for several minutes after sonication [37]. It is noteworthy that the behavioural changes that resulted from disruption of STN activity mirrored those observed in deep brain stimulation [38] and lesion studies [39]. Badran et al. [40] reported an attenuation of thermal pain sensitivity in the 10 min following an offline TUS protocol targeting the thalamus. Additional studies have linked changes in the activity of specific brain regions induced by offline TUS to variations in affect and mood [41] (and Chou et al., abstract 38 in Biological Psychiatry 2023, 93:S84-S85). It should be noted that offline TUS research in humans is still in its early stages and thus a large variability exists across studies. Factors such as stimulation parameters, control and blinding procedures, safety and transcranial acoustic simulations should be taken into consideration when interpreting study findings.

#### Clinical applications

The therapeutic potential of TUS lies in its ability to generate long-lasting changes both at the neural and behavioural levels, possibly after repeated interventions. Following the initial finding of a positive effect on mood after dorsolateral prefrontal cortex (PFC) sonication [41], the same group conducted a preclinical study with depressed participants [42]. Replicating their previous findings, they found that global affect increased over the course of the 5-day TUS intervention. However, this effect did not persist when assessed at a 1-month follow-up.

Long-term results were obtained with patients who partially recovered from a minimally conscious state after receiving thalamic ultrasound stimulation [43,44]. One patient who received ten 30-second sonications 19 days postinjury showed gradual signs of recovery starting from the day after the intervention [43]. Two of three patients in a long-lasting minimally conscious state improved after receiving two thalamic stimulation sessions of 10 min each [44]. Along with the reported antinociceptive effects of thalamic ultrasound stimulation described earlier [40], these results are encouraging for the pursuit of long-term, stable, plastic neuronal reconfiguration.

There are ongoing clinical trials testing the efficacy of TUS for the treatment of drug-resistant epilepsy [45] after its safety has been established in animal models. In a penicillin-induced epilepsy model in two nonhuman primates, offline TUS decreased the seizure frequency

and duration in both macaques for up to 7 hours after TUS [46]. A pilot study in patients with drug-resistant epilepsy [47] reported a decrease in seizure frequency in two of three patients in the 2 days following TUS of the seizure onset zone. Intracranial EEG recordings at the seizure onset zone revealed an increase in spectral power during sonication, followed by a decrease in power, for several patients. Although the authors failed to identify a link between the two measures and despite the variable response to TUS treatment, these observations also support the potential for TUS to induce neuronal plasticity.

#### Discussion on plasticity

The range of effects that has been presented in this review suggests that offline TUS can elicit long-term potentiation (LTP)-like plasticity, modifying neural circuits up to several hours after intervention. Several in vivo studies in small animals provide evidence that TUS may trigger long-lasting activity-dependent synaptic modifications through LTP and long-term depolarisation [48,49]. At the neuronal level, TUS depolarises postsynaptic neurons by activating mechanosensitive, voltage-gated sodium and calcium channels, allowing calcium influx through N-methyl-D-aspartate (NMDA) receptors [6]. This increase in postsynaptic calcium level is thought to be a key requirement for triggering changes in synaptic signalling, particularly through LTP [50]. TUS was able to restore LTP and memory in ageing mice, confirming that it can modulate NMDA receptor function [48].

With repeated treatment, offline TUS has the potential to induce long-lasting functional changes, enabling its use in clinical settings. Repetitive treatment and refinement of the dose-response relationship to induce longer-term neuroplasticity has been shown to be clinically effective in other neuromodulation techniques, such as intermittent theta-burst TMS in treatment-resistant depression [51,52]. To date, the evidence supporting long-lasting changes induced by offline TUS in primates is very limited. Of the studies we reviewed, only four found behavioural changes that persisted for several days or weeks [30,32,40,44], and in some cases, the clinical benefits later vanished [44], or in other cases, the effect of the daily stimulation decreased possibly due to adaptation [32]. Nonetheless, several studies in rodents were able to produce long-lasting behavioural changes, up to weeks, after repeated TUS treatment [48,53–55]. Combined with observations in vitro, several hypotheses regarding the downstream signalling pathway have been tested. The proposed mechanisms include (1) the action of TUS on astrocytes — mediating the synthesis and release of neurotrophic factors, such as brain-derived neurotrophic factor, (2) neurogenesis through the action of TUS on stem cells, as well as (3)

disruption of the extracellular matrix enabling synaptic reconfiguration (for a review, see Ref. [9]). Despite the recent findings in small animal studies, translating this work from rodents to primates proves to be a challenging task. Apart from differences in brain anatomy and function, the brain size, skull thickness and stimulation parameters typically employed make it difficult to compare the effectiveness of TUS between species.

#### **Conclusions**

There is some evidence that offline TUS can induce changes up to several hours after stimulation, suggesting mediation of early-phase neuroplasticity in primates. However, it remains to be understood how offline TUS — where the duration of sonication is relatively short (in the order of tens of seconds) — can lead to seemingly persistent neuronal changes in humans. It is also crucial to widen our understanding of the impact of multiple offline TUS sessions over the course of multiple weeks in terms of safety and efficacy. Therefore, understanding the neuronal reconfiguration generated by offline TUS in humans and the impact of repeated TUS interventions should be the focus of future studies to characterise its mechanism of action.

#### **Data Availability**

No data were used for the research described in the article.

#### **Declaration of Competing Interest**

The authors declare no conflict of interest.

#### **Acknowledgements**

E.F. and S.N.Y are supported by a UKRI, England Medical Research Council Future Leaders Fellowship grant MR/T023007/1 (to E.F.).

#### References and recommended reading

Papers of particular interest, published within the period of review, have been highlighted as:

- · of special interest
- of outstanding interest
- Cramer SC, Sur M, Dobkin BH, O'Brien C, Sanger TD, Trojanowski JQ, Rumsey JM, Hicks R, Cameron J, Chen D, et al.: Harnessing neuroplasticity for clinical applications. Brain 2011, **134**:1591-1609
- Palm U, Chalah MA, Ayache SS: Brain stimulation and neuroplasticity. Brain Sci 2021, 11:873.
- Bystritsky A, Korb AS, Douglas PK, Cohen MS, Melega WP Mulgaonkar AP, DeSalles A, Min B-K, Yoo S-S: A review of low-intensity focused ultrasound pulsation. *Brain Stimul* 2011,
- Gaur P, Casey KM, Kubanek J, Li N, Mohammadjavadi M, Saenz Y, Glover GH, Bouley DM, Pauly KB: Histologic safety of transcranial focused ultrasound neuromodulation and magnetic resonance acoustic radiation force imaging in rhesus macaques and sheep. Brain Stimul 2020, 13:804-814.

This paper reported an absence of tissue damage after low- and highdose ultrasound in rhesus macaque and Dorset sheep. This is an important paper to demonstrate the safety of repeated TUS.

- Attali D, Tiennot T, Schafer M, Fouragnan E, Sallet J, Caskey CF Chen R, Darmani G, Bubrick EJ, Butler C, et al.: Three-layer model with absorption for conservative estimation of the maximum acoustic transmission coefficient through the human skull for transcranial ultrasound stimulation. Brain Stimul 2023, 16:48-55.
- Yoo S, Mittelstein DR, Hurt RC, Lacroix J, Shapiro MG: Focused ultrasound excites cortical neurons via mechanosensitive calcium accumulation and ion channel amplification. Nat Commun 2022, 13:493.

The authors characterise which specific calcium-selective mechanosensitive ion channels mediate the effect of ultrasound stimulation on neurons and describe the neuronal response in response to the activation of such channels. This paper is important for understanding the biomechanisms of ultrasound modulation.

- Darmani G, Bergmann TO, Butts Pauly K, Caskey CF, de Lecea L, Fomenko A, Fouragnan E, Legon W, Murphy KR, Nandi T, *et al.*: **Non-invasive transcranial ultrasound stimulation for** neuromodulation. Clin Neurophysiol 2022, 135:51-73.
- Kop BR, Oghli YS, Grippe TC, Nandi T, Lefkes J, Meijer SW, Farboud S, Engels M, Hamani M, Null M, et al.: Auditory confounds can drive online effects of transcranial ultrasonic stimulation in humans. eLife 2023, 12:RP88762.
- Blackmore DG, Razansky D, Götz J: Ultrasound as a versatile tool for short- and long-term improvement and monitoring of brain function. Neuron 2023, 111:1174-1190.

This is a very comprehensive review, particularly for its description of the bioeffects of TUS.

10. Yaakub SN, White TA, Roberts J, Verhagen L, Stagg CJ, Hall S, Fouragnan EF: Transcranial focused ultrasound-mediated neurochemical and functional connectivity changes in deep cortical regions in humans. *Nat Commun* 2023, **14**:5318.

Using MRS and resting state functional magnetic reasonance imaging in humans, this paper shows that TUS changes overall excitability by selectively reducing GABAergic inhibition. The authors report increased connectivity of the salience network after TUS of the dorsal ACC and increased connectivity of the default mode network after TUS of the PCC

- 11. Zhang T. Guo B. Zuo Z. Long X. Hu S. Li S. Su X. Wang Y. Liu C: Excitatory-inhibitory modulation of transcranial focus ultrasound stimulation on human motor cortex. CNS Neurosci Ther 2023. 00:1-13.
- 12. Cain JA, Visagan S, Johnson MA, Crone J, Blades R, Spivak NM, Shattuck DW, Monti MM: Real time and delayed effects of subcortical low intensity focused ultrasound. Sci Rep 2021,
- 13. Kuhn T, Spivak NM, Dang BH, Becerra S, Halavi SE, Rotstein N, Rosenberg BM, Hiller S, Swenson A, Cvijanovic L, et al.: Transcranial focused ultrasound selectively increases perfusion and modulates functional connectivity of deep brain regions in humans. Front Neural Circuits 2023, 17.
- Prieto ML, Firouzi K, Khuri-Yakub BT, Madison DV, Maduke M: Spike frequency-dependent inhibition and excitation of neural activity by high-frequency ultrasound. J Gen Physiol 2020, 152:e202012672.
- 15. Dong S, Xie Z, Yuan Y: Transcranial ultrasound stimulation modulates neural activities during NREM and REM depending on the stimulation phase of slow oscillations and theta waves in the hippocampus. Cereb Cortex 2023, 33:8956-8966.
- Samuel N, Zeng K, Harmsen IE, Ding MYR, Darmani G, Sarica C, Santyr B, Vetkas A, Pancholi A, Fomenko A, et al.: Multi-modal investigation of transcranial ultrasound-induced neuroplasticity of the human motor cortex. Brain Stimul 2022, 15:1337-1347.
- Mars RB, Verhagen L, Gladwin TE, Neubert F-X, Sallet J, Rushworth MFS: Comparing brains by matching connectivity profiles. Neurosci Biobehav Rev 2016, 60:90-97.

- 18. Mars RB, Sotiropoulos SN, Passingham RE, Sallet J, Verhagen L, Khrapitchev AA, Sibson N, Jbabdi S: Whole brain comparative anatomy using connectivity blueprints. eLife 2018, 7:e35237.
- 19. Verhagen L, Gallea C, Folloni D, Constans C, Jensen DE, Ahnine H, Roumazeilles L, Santin M, Ahmed B, Lehericy S, et al.: Offline impact of transcranial focused ultrasound on cortical activation in primates. eLife 2019, 8:e40541.
- Folloni D, Verhagen L, Mars RB, Fouragnan E, Constans C, Aubry
   J-F, Rushworth MFS, Sallet J: Manipulation of subcortical and deep cortical activity in the primate brain using transcranial focused ultrasound stimulation. Neuron 2019, 101:1109-1116 e5. Using resting-state fMRI, these two papers show how TUS modifies the connectional fingerprint of the cortical and subcortical stimulated area

with high specificity. 21. Liu D, Munoz F, Sanatkhani S, Pouliopoulos AN, Konofagou E, Grinband J, Ferrera V: **Alteration of functional connectivity in the** cortex and major brain networks of non-human primates

- following focused ultrasound exposure. Brain Stimul 2023, **16**:1196-1204
- 22. Zhang Y, Ren L, Liu K, Tong S, Yuan T-F, Sun J: Transcranial ultrasound stimulation of the human motor cortex. iScience 2021. 24:103429.
- 23. Zeng K, Darmani G, Fomenko A, Xia X, Tran S, Nankoo J-F, Shamli Oghli Y, Wang Y, Lozano AM, Chen R: Induction of human motor cortex plasticity by theta burst transcranial ultrasound stimulation. Ann Neurol 2022, 91:238-252.
- 24. Ren L, Zhai Z, Xiang Q, Zhuo K, Zhang S, Zhang Y, Jiao X, Tong S, Liu D, Sun J: Transcranial ultrasound stimulation modulates the interhemispheric balance of excitability in human motor cortex. J Neural Eng 2023, 20:016043.
- 25. Bergmann TO, Hartwigsen G: Inferring causality from noninvasive brain stimulation in cognitive neuroscience. J Cogn Neurosci 2021, 33:195-225.
- 26. Bongioanni A, Folloni D, Verhagen L, Sallet J, Klein-Flügge MC, Rushworth MFS: Activation and disruption of a neural mechanism for novel choice in monkeys. Nature 2021, **591**:270-274.
- 27. Folloni D, Fouragnan E, Wittmann MK, Roumazeilles L, Tankelevitch L, Verhagen L, Attali D, Aubry J-F, Sallet J, Rushworth MFS: Ultrasound modulation of macaque prefrontal cortex selectively alters credit assignment-related activity and behavior. Sci Adv 2021, 7:eabg7700.

Using event-related fMRI in awake macagues, the authors show that TUS of area 47/12o, and not the frontal pole, selectively change neural activity and behaviour related to both reward-based learning and valuebased decision making

- Fouragnan EF, Chau BKH, Folloni D, Kolling N, Verhagen L, Klein-Flügge M, Tankelevitch L, Papageorgiou GK, Aubry J-F, Sallet J, et al.: The macaque anterior cingulate cortex translates counterfactual choice value into actual behavioral change. Nat Neurosci 2019, 22:797-808.
- 29. Khalighinejad N, Bongioanni A, Verhagen L, Folloni D, Attali D, Aubry J-F, Sallet J, Rushworth MFS, Basal Forebrain-Cingulate A: Circuit in macaques decides it is time to act. Neuron 2020, 105:370-384 e8..
- 30. Munoz F, Meaney A, Gross A, Liu K, Pouliopoulos AN, Liu D,
   Konofagou EE, Ferrera VP: Long term study of motivational and cognitive effects of low-intensity focused ultrasound neuromodulation in the dorsal striatum of nonhuman primates. Brain Stimul 2022, 15:360-372.

This was the first paper to report lasting behavioural and neuronal effects of repeated TUS in nonhuman primates, over several months. This is also an important paper for safety aspects.

31. Pouget P, Frey S, Ahnine H, Attali D, Claron J, Constans C, Aubry J-F, Arcizet F: Neuronavigated repetitive transcranial ultrasound stimulation induces long-lasting and reversible effects on oculomotor performance in non-human primates. Front Physiol 2020, 11:1042.

•• modulation of primate deep brain circuits with focused ultrasonic waves. Brain Stimul 2023, 16:798-805.

In this study, ultrasound was delivered daily for a period of 6 months into deep brain structures of nonhuman primates. In addition to behavioural effects, the authors report the results from intracranial recordings.

- Ai L, Bansal P, Mueller JK, Legon W: Effects of transcranial focused ultrasound on human primary motor cortex using 7T fMRI: a pilot study. BMC Neurosci 2018, 19:56.
- 34. Fomenko A, Chen K-HS, Nankoo J-F, Saravanamuttu J, Wang Y, El-Baba M, Xia X, Seerala SS, Hynynen K, Lozano AM, et al.: Systematic examination of low-intensity ultrasound parameters on human motor cortex excitability and behavior. eLife 2020, 9:e54497.
- 35. Butler CR, Rhodes E, Blackmore J, Cheng X, Peach RL, Veldsman M. Sheerin F. Cleveland RO: Transcranial ultrasound stimulation to human middle temporal complex improves visual motion detection and modulates electrophysiological responses. Brain Stimul 2022. 15:1236-1245.
- 36. Legon W, Sato TF, Opitz A, Mueller J, Barbour A, Williams A, Tyler WJ: Transcranial focused ultrasound modulates the activity of primary somatosensory cortex in humans. Nat Neurosci 2014, **17**:322-329.
- 37. Nakajima K, Osada T, Ogawa A, Tanaka M, Oka S, Kamagata K, Aoki S, Oshima Y, Tanaka S, Konishi S: A causal role of anterior prefrontal-putamen circuit for response inhibition revealed by transcranial ultrasound stimulation in humans. Cell Rep 2022,
- 38. Lofredi R, Auernig GC, Irmen F, Nieweler J, Neumann W-J, Horn A, Schneider G-H, Kühn AA: Subthalamic stimulation impairs stopping of ongoing movements. Brain 2021, 144:44-52.
- 39. Obeso I, Wilkinson L, Casabona E, Speekenbrink M, Luisa Bringas M, Álvarez M, Álvarez L, Pavón N, Rodríguez-Oroz MC, Macías R, et al.: The subthalamic nucleus and inhibitory control: impact of subthalamotomy in Parkinson's disease. Brain 2014, **137**:1470-1480.
- Badran BW, Caulfield KA, Stomberg-Firestein S, Summers PM, Dowdle LT, Savoca M, Li X, Austelle CW, Short EB, Borckardt JJ, et al.: Sonication of the anterior thalamus with MRI-Guided transcranial focused ultrasound (tFUS) alters pain thresholds in healthy adults: a double-blind, sham-controlled study. Brain Stimul 2020, 13:1805-1812.
- 41. Sanguinetti JL, Hameroff S, Smith EE, Sato T, Daft CMW, Tyler WJ, Allen JJB: Transcranial focused ultrasound to the right prefrontal cortex improves mood and alters functional connectivity in humans. Front Hum Neurosci 2020, 14.
- 42. Reznik SJ, Sanguinetti JL, Tyler WJ, Daft C, Allen JJB: A doubleblind pilot study of transcranial ultrasound (TUS) as a five-day intervention: TUS mitigates worry among depressed participants. Neurol Psychiatry Brain Res 2020, 37:60-66.
- 43. Monti MM, Schnakers C, Korb AS, Bystritsky A, Vespa PM: Noninvasive ultrasonic thalamic stimulation in disorders of

- consciousness after severe brain injury: a first-in-man report. Brain Stimul 2016, 9:940-941.
- 44. Cain JA, Spivak NM, Coetzee JP, Crone JS, Johnson MA Lutkenhoff ES, Real C, Buitrago-Blanco M, Vespa PM, Schnakers C, et al.: Ultrasonic thalamic stimulation in chronic disorders of consciousness. Brain Stimul 2021, 14:301-303.
- 45. Bubrick EJ, McDannold NJ, White PJ: Low intensity focused ultrasound for epilepsy — a new approach to neuromodulation. Epilepsy Curr 2022,156-160, https://doi.org/10.1177/ 15357597221086111
- 46. Zou J, Meng L, Lin Z, Qiao Y, Tie C, Wang Y, Huang X, Yuan T, Chi Y, Meng W, et al.: Ultrasound neuromodulation inhibits seizures in acute epileptic monkeys. iScience 2020, 23:101066.
- 47. Lee C-C, Chou C-C, Hsiao F-J, Chen Y-H, Lin C-F, Chen C-J, Peng S-J, Liu H-L, Yu H-Y: Pilot study of focused ultrasound for drugresistant epilepsy. Epilepsia 2022, 63:162-175.
- **48.** Blackmore DG, Turpin F, Palliyaguru T, Evans HT, Chicoteau A, Lee W, Pelekanos M, Nguyen N, Song J, Sullivan RKP, *et al.*: **Low**intensity ultrasound restores long-term potentiation and memory in senescent mice through pleiotropic mechanisms including NMDAR signaling. Mol Psychiatry 2021, 26:6975-6991.
- 49. Oh S-J, Lee JM, Kim H-B, Lee J, Han S, Bae JY, Hong G-S, Koh W, Kwon J, Hwang E-S, et al.: Ultrasonic neuromodulation via astrocytic TRPA1. Curr Biol 2019, 29:3386-3401 e8.
- 50. Citri A, Malenka RC: Synaptic plasticity: multiple forms, functions, and mechanisms. Neuropsychopharmacology 2008, **33**:18-41.
- 51. Cole EJ, Stimpson KH, Bentzley BS, Gulser M, Cherian K, Tischler C, Nejad R, Pankow H, Choi E, Aaron H, et al.: Stanford accelerated intelligent neuromodulation therapy for treatmentresistant depression. Am J Psychiatry 2020, 177:716-726.
- 52. Cole EJ, Phillips AL, Bentzley BS, Stimpson KH, Nejad R, Barmak F, Veerapal C, Khan N, Cherian K, Felber E, et al.: Stanford neuromodulation therapy (SNT): a double-blind randomized controlled trial. Am J Psychiatry 2022, 179:132-141.
- 53. Shen Y, Hua L, Yeh C-K, Shen L, Ying M, Zhang Z, Liu G, Li S, Chen S, Chen X, et al.: Ultrasound with microbubbles improves memory, ameliorates pathology and modulates hippocampal proteomic changes in a triple transgenic mouse model of Alzheimer's disease. Theranostics 2020, 10:11794-11819.
- 54. Eguchi K, Shindo T, Ito K, Ogata T, Kurosawa R, Kagaya Y, Monma Y, Ichijo S, Kasukabe S, Miyata S, et al.: Whole-brain lowintensity pulsed ultrasound therapy markedly improves cognitive dysfunctions in mouse models of dementia - crucial roles of endothelial nitric oxide synthase. Brain Stimul 2018,
- 55. Blackmore DG, Turpin F, Mohamed AZ, Zong F, Pandit R, Pelekanos M, Nasrallah F, Sah P, Bartlett PF, Götz J: **Multimodal** analysis of aged wild-type mice exposed to repeated scanning ultrasound treatments demonstrates long-term safety. Theranostics 2018, 8:6233-6247.